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## Multicolor two-photon light-sheet microscopy

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Two-photon microscopy is the most effective approach for deep-tissue fluorescence cellular imaging; however, its application to high-throughput or high-content imaging is often hampered by low pixel rates, challenging multicolor excitation and potential cumulative photodamage. To overcome these limitations, we extended our prior work and combined two-photon scanned light-sheet illumination (or two-photon selective-plane illumination microscopy, 2P-SPIM)<sup>1</sup> with mixed-wavelength excitation<sup>2</sup> to achieve fast multicolor two-photon imaging with negligible photobleaching compared to conventional two-photon laser point-scanning microscopy (2P-LSM). We report on the implementation of this strategy and, to illustrate its potential, recorded sustained four-dimensional (4D: three dimensions + time) multicolor two-photon movies of the beating heart in zebrafish embryos at 28-MHz pixel rates.

To obtain multicolor two-photon excitation by wavelength mixing, we spatially and temporally overlapped two pulse trains produced by a femtosecond laser and an optical parametric oscillator (**Fig. 1a**). The two beams separately generate two-photon-excited fluorescence (2PEF; **Fig. 1a**) of blue and red chromophores, and their spatiotemporal overlap provides an additional two-photon excitation route to probe a third chromophore (i.e., in the green-yellow range) through twocolor two-photon-excited fluorescence<sup>2</sup> (2C-2PEF; **Fig. 1a**). To implement this multicolor strategy, we added an optical parametric oscillator, a delay line and a spectral image splitter to a bidirectional 2P-SPIM setup (**Fig. 1b**, **Supplementary Fig. 1** and **Supplementary Methods**). Implementation of wavelength mixing in the 2P-SPIM geometry differs from the 2P-LSM case in several ways, including the orthogonal configuration of excitation and detection axes, weakly focused excitation, bidirectional illumination and camera-based wide-field detection in 2P-SPIM (**Supplementary Methods**). We temporally synchronized the two pulse trains in both illumination paths by matching their chromatic dispersion (**Supplementary Fig. 2**). In turn, the reduced sensitivity to illumination chromatic aberration in 2P-SPIM enabled us to straightforwardly achieve spatial overlapping of the two beams and wavelength mixing over a larger field of view than is possible with 2P-LSM (**Supplementary Fig. 3**). Overall, we obtained efficient implementation of mixed-wavelength 2P-SPIM with bidirectional illumination, as illustrated by simultaneous trichromatic two-photon imaging of fly embryos (**Fig. 1c**).

Sustained two-photon excitation of multiple fluorescent proteins is limited by photobleaching: for instance, illumination in the 800-nm-wavelength range required for blue fluorophore excitation increases the photobleaching rate of red fluorescent proteins<sup>3</sup> (**Supplementary Fig. 4**). To compare the photobleaching induced by multicolor 2P-SPIM and 2P-LSM when using mixed-wavelength excitation, we recorded images of live fly embryos with both microscopes using similar acquisition parameters (acquisition time, average power, signal level and spatial resolution; **Supplementary Table 1**). Multicolor 2P-SPIM induced substantially lower photobleaching than did 2P-LSM: we observed a 25-fold decrease for 2PEF of RFP and undetectable photobleaching for 2C-2PEF of GFP (**Fig. 1d**, **Supplementary Fig. 4** and **Supplementary Methods**). When both methods are set up so as to obtain comparable fluorescence signal levels, reduced photobleaching in multicolor 2P-SPIM originates from lower peak intensities and different illumination dynamics relative to those of 2P-LSM<sup>1,4</sup>. As a consequence, multicolor 2P-SPIM allows the use of higher average powers to improve signal-to-noise ratio or increase imaging speed.

Finally, to demonstrate high-speed multicolor two-photon imaging, we recorded 3D time-lapse images of the beating heart in zebrafish embryos exhibiting CFP, GFP and DsRed labeling of pericardial, myocardial and red blood cells, respectively (**Supplementary Methods** and **Supplementary Table 2**). We acquired fast time series of multicolor two-photon images (up to 85 frames/s and 28 million pixels/s) at successive depths allowing 3D reconstruction of the heart periodic motion<sup>5</sup> (**Fig. 1e,f**, **Supplementary Video 1** and **Supplementary Methods**). Notably, multicolor 2P-SPIM imaging of the beating heart did not induce detectable photodamage (**Supplementary Fig. 5**) and provided 2C-2PEF signal with sufficient spatiotemporal resolution for quantitative 3D tracking of myocardial cells moving at up to 600  $\mu\text{m/s}$  within the entire heart (**Fig. 1g** and **Supplementary Video 2**).

The combination of mixed-wavelength excitation with light-sheet illumination provides a robust and efficient way to achieve multicolor two-photon tissue imaging at high pixel rates and signal levels while dramatically reducing photobleaching. This strategy should prove invaluable in systems biology.

Note: Any Supplementary Information and Source Data files are available in the online version of the paper (doi:10.1038/nmeth.2963).

## ACKNOWLEDGMENTS

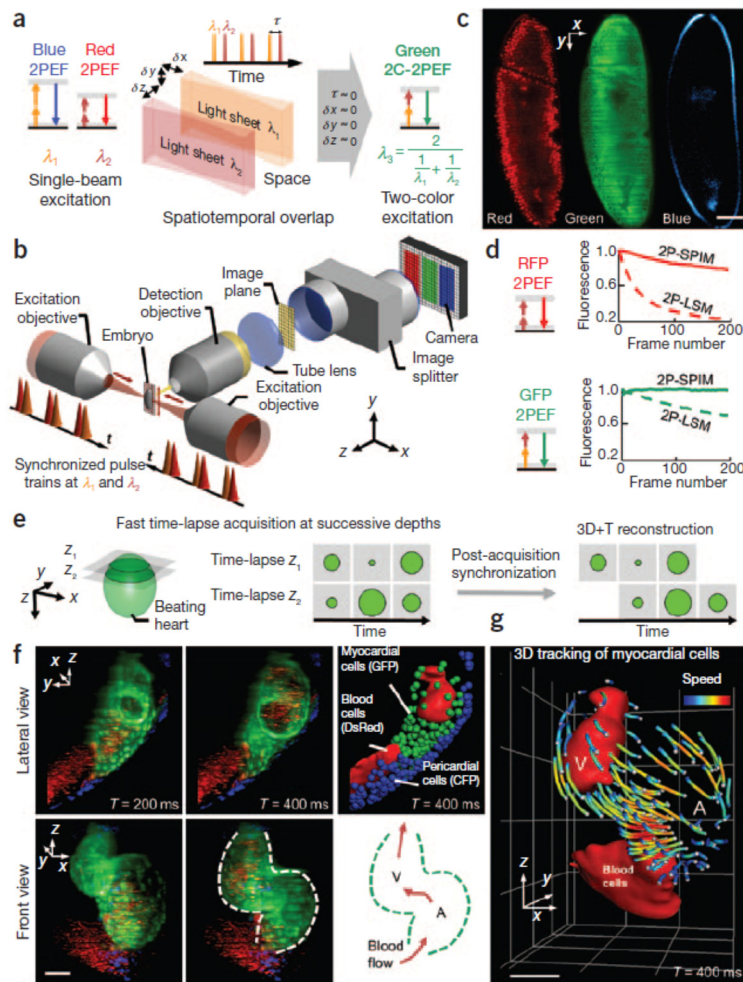
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## AUTHOR CONTRIBUTIONS

P.M., E.B. and W.S. conceived of the project and implemented the optical setup. P.M. and W.S. performed fly and zebrafish imaging and image analysis. J.V. provided and labeled the zebrafish lines. P.M., E.B. and W.S. wrote the manuscript.

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**Figure 1** | Fast trichromatic two-photon imaging of live embryos using mixed-wavelength light-sheet excitation. **(a)** Principles of mixed wavelength excitation in 2P-SPIM geometry. **(b)** Optical setup of a multicolor 2P-SPIM microscope with bidirectional illumination. Two synchronized femtosecond pulse trains ( $\lambda_1 = 820\text{--}840\text{ nm}$  and  $\lambda_2 = 1,090\text{--}1,175\text{ nm}$ ) are vertically scanned at the foci of two low-numerical aperture (NA) objectives to create bidirectional light-sheet illumination. The image is collected by an orthogonal detection objective, and spectral components are spatially separated on an electron-multiplying charge-coupled device (EMCCD) camera by an image splitter. **(c)** Simultaneous trichromatic 2PEF imaging of a GFP- and RFP-labeled gastrulating fly embryo showing endogenous signal from the yolk and the vitelline membrane (blue), green labeling of the cell membranes and red labeling of the nuclei. **(d)** Reduced photobleaching of RFP and GFP using 2P-SPIM compared to 2P-LSM with similar acquisition parameters (see **Supplementary Fig. 4**). **(e–g)** Fast multicolor 2P-SPIM imaging of a zebrafish embryo heart at 2 d post fertilization and exhibiting CFP, GFP and DsRed labeling of nuclei, myocardial cells and red blood cells, respectively. **(e)** 2D series are recorded at a rate of 48–85 frames/s in successive planes with no appreciable bleaching, and the periodic contractions are reconstructed in three dimensions using post-processing synchronization with typically 0.4-μm lateral and 3-μm axial optical resolution within a  $210 \times 230 \times 300\text{ }\mu\text{m}^3$  acquisition volume and the  $0.67 \times 0.67 \times 2.0\text{ }\mu\text{m}^3$  voxel size (**Supplementary Videos 1 and 2** and **Supplementary Methods**). **(f,g)** 2C-2PEF signal from GFP-labeled myocardial cells **(f)** is sufficient for 3D cell tracking **(g)**. V, ventricle; A, atrium. Color-coded speed ranges from 0 to 620 μm/s; grid spacing is 67 μm. Scale bars, 50 μm.